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Flow-cell device.

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THE JOURNAL OF HISTOCHEMISTRY AND CYTOCHEMISTRY vol. 25, no. 7, 1977, pages 774-780; V. KACHEL et al.: "Uniform Lateral Orientation, caused by flow forces, of flat particles in flow through systems"

REVIEW OF SCIENTIFIC INSTRUMENTS vol. 55, no. 9, September 1984, pages 1375-1400, New York, US; J.A. STEINKAMP: "Flow cytometry"

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Description

BACKGROUND OF THE INVENTION

The present invention relates to a flow-cell device and, more particularly, to a flow-cell device suitable for use in cellular analysis of living bodies.

Hitherto, apparatus has been known for conducting cellular analysis of living bodies by causing cells extracted from a living body to flow in a flow-cell device while effecting photometry of the cells. In this apparatus, generally known as Flow-Cytometer, a light beam is applied to cells in the suspension of cells and on the basis of scattering light and fluorescence from the cells, the analyses of the sizes, shapes and other state of cells are conducted.

In operation of the flow-cytometer, in order to pour the suspension of cells through a capillary flow passage for measurement in stable and without clogging, a method has been adopted in which the suspension of cells is made to flow by being surrounded by physiological saline. The method will be described with reference to Fig. 10. Fig. 10 shows a concept of the method. In Fig. 10, the suspension of cells 1, namely, sample fluid is surrounded by the physiological saline 2, namely, sheath fluid. That is, sheath fluid flow is formed around sample fluid flow and the sample fluid flow becomes a laminar flow. The sample fluid and the sheath fluid are discharged from a discharge port 3 to the exterior.

This method is referred to as "sheath-flow method", and constitutes an effective measure in the cellular analysis, but involves the following disadvantages. Forces 4 as shown in Fig. 10 act on the cells in the suspension from the surfaces of the capillary flow passage surfaces and physiological saline, so that flat cells such as red corpuscle are oriented at random in the measuring portion, with the result that the measurement data of scattered lights and fluorescence fluctuate undesirably.

Two measures have been taken for the purpose of overcoming these problems. One of these measures is to introduce a variation in the length-to-breadth ratio between the flow-contracting portion and the capillary flow passage as shown in Fig. 11, so as to vary the magnitudes of the forces acting on the flowing cells in the longitudinal and breadthwise directions, thereby to uniformly orient the flat cells. This method is discussed in the Journal of Histochemistry and Cytochemistry, Vol. 25, No. 7 (1977) pp. 774-780.

Another measure is to adopt a wedge-shaped form on the end of a nozzle 5 through which the suspension of cells (sample fluid) is discharged into the flow of the sheath fluid, as shown in Figs. 12A and 12B. Fig. 12A is a perspective view of the

nozzle 5. Fig. 12B is a sectional view of the flow-cell showing the state of flow of the sample fluid 1 and the sheath fluid 2 supplied from the nozzle 5. As shown in Figs. 12A and 12B, by using a wedge-shaped form on the end of the nozzle 5, the sample fluid flow in the sheath fluid flow becomes flat. Therefore, it is possible to confine the flat cells in the flat flow of the sample fluid. This method is described in detail in "Biophysics Journal", Vol. 23 (1978) pp. 7-13.

An apparatus for such a measurement is described in U.S.-A-3,893,766. The flow chamber in this document operates with a symmetrical velocity distribution over the flow channel.

Another apparatus for measuring special properties of particles suspended in a fluid is described in EP-A-0 163 206. In this apparatus a sheath fluid surrounds a sample fluid at three sides so that the sample fluid flows on the sheath fluid. This apparatus too works with a symmetrical velocity profile of the fluid in the measuring area.

The prior arts described involve the following problems. Namely, in the method of Fig. 11 relying upon variation of the length-to-breadth ratio of the cross-section of the flow-cell, the ratio between the forces acting on the cell in the longitudinal and breadthwise directions is constant, so that the cell receives rotational moment depending on the initial posture of the cell discharged from the nozzle. In consequence, the cells fail to be oriented in the same direction.

On the other hand, the known arts relying upon wedge-shaped form of the suspension explained with reference to Figs. 12A and 12B has a drawback in that the flattened flow of the suspension tends to be twisted in the form of a ribbon, even by a slight turbulence of the sheath fluid (physiological saline), with the result that the measurement of the flat cells in the constant direction is failed.

Obviously, the fact that the flat cells cannot be measured stably in flat positions impairs the precision of the data obtained through the measurement conducted at the photometry section.

SUMMARY OF THE INVENTION

Accordingly, an object of the present invention is to provide a flow-cell device which enables highly accurate photometry of cells even the cells are flat.

According to the present invention, there is provided a sheath flow type flow-cell device for flow-cytometer as defined in claim 1, 6 or 7.

In the flow-cell device of the present invention, the flow of fluid in the capillary flow passage takes the form of parallel flows having a certain velocity gradient, i.e., the form of a sheared flow, so that

the cells existing in the sheared flow are deformed to assume shapes symmetrical with respect to their axes, whereby the flat cells are oriented in the same posture, thus avoiding any fluctuation of the photometric data and, hence, assuring high precision of measurement.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 is a sectional plan view of an embodiment of the flow-cell device in accordance with the present invention;

Fig. 2 is a sectional view taken along the line II-II of Fig. 1;

Fig. 3 is an enlarged view of a portion marked at A in Fig. 1;

Fig. 4 is an enlarged view of a portion marked at B in Fig. 3;

Fig. 5 is a sectional view taken along the line V-V of Fig. 3;

Fig. 6 is a sectional view showing the modification of the embodiment shown in Fig. 5;

Fig. 7 is an enlarged view similar to that in Fig. 3, illustrating another embodiment of the flow-cell device in accordance with the present invention;

Fig. 8 is a sectional view taken along the line VII-VII of Fig. 7;

Fig. 9 is an enlarged view similar to that in Fig. 3, illustrating another embodiment of the flow-cell device in accordance with the present invention;

Fig. 10 is a schematic illustration of a prior art flow-cell device;

Fig. 11 is a sectional view of another prior art flow-cell device;

Fig. 12A is a perspective view of a nozzle used in a prior-art flow-cell device; and

Fig. 12B is a sectional view of the flow cell device incorporating the nozzle shown in Fig. 12A.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

Preferred embodiments of the present invention will be described hereinafter with reference to the accompanying drawings. Fig. 1 shows an embodiment of the flow-cell device of the invention. The flow-cell device has a first inlet 6 for sheath fluid 2, a second inlet 7 for suspension of cells 1 (referred to as "sample fluid", hereinafter), a flow passage 9 communicating with the first inlet 6 and contracting downward, a straight capillary flow passage 8 communicating with the flow passage 9 at an end of the latter, a discharge port 3 provided at a terminal end of the capillary flow passage 8, and a nozzle 10 opened in the flow passage 9. The

nozzle 10 is opened in the same direction as the direction of flow of the sample fluid in the capillary flow passage 8. The capillary flow passage 8 and the flow passage 9 have substantially rectangular cross-sections. The top wall 15 and the bottom wall 16 of the capillary flow passage 8 are made transparent so that measuring light can pass therethrough.

The capillary flow passage 8 is provided with flow regulating means. Namely, one 8a of the side wall of the capillary flow passage has a smooth surface, while the other side wall 8b has roughened surface. In consequence, the fluid flowing through the capillary flow passage 8 encounters comparatively small resistance at its portion adjacent to the smooth surface and comparatively large resistance at its portion adjacent to the roughened surface. The distance between the side wall 8a and the side wall 8b is usually as small as 50 μm to 500 μm . Therefore, the flow of the fluid in the capillary flow passage 8 forms a sheared flow. Namely, the flow of the fluid in the capillary flow passage 8 is a laminar flow having a velocity gradient pattern 14 shown in Fig. 4.

The operation of this embodiment is as follows.

The nozzle 10 is supplied with a sample fluid 1 which is a suspension fluid including cells 13 to be examined. The sample fluid is fed under pressure so that a flow of the sample fluid occurs in the capillary flow passage 8 from the end of the nozzle 10. Meanwhile, a sheath fluid 2 is fed under pressure in the flow passage 9 around the nozzle 10. Thus, the sheath fluid 2 flows in such a manner that it surrounds or sheathes the sample fluid 1. At the same time, the flow passage 9 leading to the measuring section is contracted to a predetermined size. For these reasons, the sample fluid 1 is drastically contracted to form a contracted laminar flow. As a result, cells are made to pass through the measuring section in a one-by-one fashion. The flow of the fluid in the capillary flow passage 8 is a laminar flow having a velocity gradient, i.e., a sheared flow. The cell 13 subjected to the sheared flow, therefore, is deformed into a cell 2 which has a form symmetrical with respect to the axis thereof. Thus, the cell 2 becomes to have a form resembling that of a Rugby ball with its longitudinal axis coinciding with the direction of the flow. As a result, all the cells, even if they may be flat, take the same posture when they pass through the measuring section, whereby any fluctuation of the measured data is avoided to ensure a high degree of precision of measurement.

Regarding the degree of smoothness of the surfaces of the side walls, the roughness of the smooth surface is not greater than 1/500 of the distance between the side wall surfaces, while the roughness of the roughened surface is preferably

1/20 or greater of the distance between the side wall surfaces. More specifically, the roughness of the smooth wall surface ranges between 1S and 10S, while the roughness of the roughened surface ranges between 100S and 1000S.

Fig. 6 shows a modification of the embodiment described above. In this embodiment, the roughened surface extends to constitute parts of the top wall 15 and the bottom wall 16. With this arrangement, the laminar flow of the fluid in the capillary flow passage 8 can have a greater velocity gradient than that in the embodiment shown in Fig. 5. This means that the modification shown in Fig. 6 promotes the tendency for the cell to assume a form which is symmetrical with respect to its axis, as compared to the case of the embodiment shown in Fig. 1.

Obviously, the described embodiment of the present invention should be designed to enable measurement of scattered light and fluorescence through the transparent top wall 15 and the bottom wall 16. The width of the roughened regions 17, 18 on the top wall and the bottom wall, therefore, should be not greater than 1/3 that of the distance between the opposing side walls, in order to enable such measurement. It is also necessary that the optical system be adjusted so as to prevent incident light and the scattered light from impinging upon these regions.

In the embodiment shown in Figs. 1 and 6, the smoothness of the smooth wall surface may be formed by polishing, plating or any other known suitable method. The roughening of the surfaces may be done by knurling or fine cutting or the like.

Another embodiment of the present invention will be described with reference to Figs. 7 and 8. A net member 19 is disposed upstream from the opening of the nozzle 10 across the flow passage 9. The mesh of the net is so varied that it becomes finer from one 21 of the side walls towards the other 22. In consequence, the sheath fluid flowing in the flow passage 9 encounters resistance which varies along the plane of the net member 19 in accordance with the variation of the mesh. In consequence, the fluid flowing in the capillary flow passage exhibits a flow velocity distribution pattern as shown in Fig. 4, thereby the cells are deformed into a form which is symmetrical with respect to the axis thereof. In this embodiment, it is not preferred to dispose the net member 19 downstream from the end of the nozzle 10, because in such a case the cells 13 will be undesirably caught by the mesh of the net member 19 to hinder the measurement.

Another embodiment of the present invention will be described hereinafter with reference to Fig. 9.

In the embodiment, a plurality of partition walls 20 extending in the flow direction of the flow passage 9 are provided in the flow passage 9. The partition walls 20 divide the flow passage 9 into a plurality of divided flow passages. In the illustrated case, the flow passage 9 is divided into six divided flow passages 23a, 23b, 23c, 23d, 23e, 23f. The length of the divided flow passages are made longer as the divided flow passages locate near the side wall 21. Therefore, the flow resistance of the divided flow passages 23a, 23b, 23c, 23d, 23e, 23f are larger as they locate near the side wall 21, whereby a flow velocity distribution pattern of the sheath fluid as shown in Fig. 4 is obtained. As a result, it is possible to deform the cells in the sample fluid flowing through the capillary flow passage 8 into the form which is symmetrical with respect to its longitudinal axis. The number of the partition walls may be varied as desired.

As described hereinbefore, according to the present invention, the fluid flowing through the capillary flow passage forms a sheared flow over the entire cross-section of the capillary flow passage. As a result, the cells in the sample fluid is deformed into a form which is in symmetry with respect to its axis. This ensures that all cells, even if they may be flat, are oriented in the constant direction so as to eliminate any fluctuation of the measured data.

Claims

1. A sheath flow type flow-cell device for a flow-cytometer comprising:
 - a first inlet (6) for sheath fluid,
 - a first flow passage (9) communicating with said first inlet (6) and contracted toward downstream, said first flow passage (9) having a substantially rectangular cross section and opposing first and second side walls (8a, 8b) connected by top and bottom walls (15, 16) the top wall being transparent and designed to enable measurement of scattered light and fluorescence therethrough,
 - a second straight capillary flow passage (8) connected to said first flow passage (9) at downstream thereof, said second capillary flow passage (8) having a substantially rectangular cross section,
 - a second inlet (7) for sample fluid,
 - a nozzle (10) communicating with said second inlet (7) and opening within said first flow passage (9) in the same direction as the flow direction of said second straight capillary flow passage (8),
 - a discharge port (3) provided at a terminal end of said second straight capillary flow passage (8),

characterized by

flow regulating means for regulating the flow of said sheath fluid in said second capillary flow passage (8) to be a laminar flow having a gradient of flow velocity across said second straight capillary flow, said velocity decreasing passage (8) from said first side wall (8a) to said second side wall (8b), wherein said flow regulating means comprises said second side wall (8b) having a rougher surface than a surface of said first side wall (8a).

2. A sheath flow type flow-cell device as claimed in claim 1, wherein said flow regulating means further includes a part (17) of said top wall (15) and a part (18) of said bottom wall (16) of said second capillary flow passage (9) having rough surface portions adjacent to said second side wall (8b).
3. A sheath flow type flow-cell device as claimed in claim 1, wherein the surface roughness of said surface of said first side wall (8a) is 1/500 and under of a distance between said first side wall (8a) and said second side wall (8b) and the surface roughness of said surface of said second side wall (8b) is 1/20 and over of said distance.
4. A sheath flow type flow-cell device as claimed in claim 1, wherein the surface roughness of said surface of said first side wall (8a) exists from 1S to 10S and the surface roughness of said surface of said second side wall (8b) exists from 100S to 1000S.
5. A sheath flow type flow-cell device as claimed in claim 2, wherein the width of said rough surfaces (17, 18) of said top and bottom walls (15, 16) from said second side wall (8b) is 1/3 and under of a distance between said first side wall (8a) and said second side wall (8b).
6. A sheath flow type flow-cell device for a flow-cytometer comprising:
 - a first inlet (6) for sheath fluid,
 - a first flow passage (9) communicating with said first inlet (6) and contracted toward downstream, said first flow passage (9) having a substantially rectangular cross section and opposing first and second side walls (21, 22) connected by top and bottom walls the top wall being transparent and designed to enable measurement of scattered light and fluorescence therethrough,
 - a second straight capillary flow passage (8) connected to said first flow passage (9) at downstream thereof, said second capillary flow

passage (8) having a substantially rectangular cross section,
 a second inlet (7) for sample fluid,
 a nozzle (10) communicating with said second inlet (7) and opened within said first flow passage (9) in the same direction as the flow direction of said second straight capillary flow passage (8),
 a discharge port (3) provided at a terminal end of said second straight capillary flow passage (8),

characterized by

flow regulating means for regulating the flow of said sheath fluid in said second straight capillary flow passage (8) to be a laminar flow having a gradient of flow velocity across said second straight capillary, said velocity decreasing flow passage from said first side wall (21) to said second side wall (22), wherein said flow regulating means comprises a net member (19) stretched across said first flow passage (9) upstream from the opening of said nozzle (10), the mesh of said net member (19) being minuter from said first side wall (21) of said first flow passage (9) toward said second side wall (22) opposite to said first side wall (21).

7. A sheath flow type flow-cell device for a flow-cytometer comprising:
 - a first inlet (6) for sheath fluid,
 - a first flow passage (9) communicating with said first inlet (6) and contracted toward downstream, said first flow passage (9) having a substantially rectangular cross section and opposing first and second side walls (22, 21) connected by top and bottom walls the top wall being transparent and designed to enable measurement of scattered light and fluorescence therethrough,
 - a second straight capillary flow passage (8) connected to said first flow passage (9) at downstream thereof, said second capillary flow passage (8) having a substantially rectangular cross section,
 - a second inlet (7) for sample fluid,
 - a nozzle (10) communicating with said second inlet (7) and opened within said first flow passage (9) in the same direction as the flow direction of said second straight capillary flow passage (8),
 - a discharge port (3) provided at a terminal end of said second capillary flow passage (8),
- characterized by**
- flow regulating means for regulating the flow of said sheath fluid in said second straight capillary flow passage (8) to be a laminar flow having a gradient of flow velocity across said

straight capillary, said velocity decreasing flow passage from said first side wall (22) to said second side wall (21), wherein said flow regulating means comprises a plurality of partition walls (20) extending in said first flow passage (9) in the flow direction and dividing it into a plurality of divided flow passages (23a, 23b, 23c, 23d, 23e, 23f) the lengths of which are made larger from said first side wall (22) of said first flow passage (9) toward said second side wall (21) opposite to said first side wall (22) to make flow resistance larger from said first side wall (22) toward said second side wall (21).

Patentansprüche

1. Durchflußzellenvorrichtung des Mantelströmungstyps für ein Strömungs-Zytometer, die aufweist:
einen ersten Einlaß (6) für ein Mantelfluid;
einen ersten Strömungsdurchgang (9), der mit dem ersten Einlaß (6) kommuniziert und stromabwärts zusammengezogen ist, wobei der erste Strömungsdurchgang (9) einen im wesentlichen rechteckigen Querschnitt und gegenüberliegende erste und zweite Seitenwände (8a, 8b) aufweist, die durch obere und Bodenwände (15, 16) verbunden sind, wobei die obere Wand transparent ist und so ausgelegt ist, daß durch sie eine Messung von Streulicht und Fluoreszenz ermöglicht ist,
einen zweiten geraden kapillaren Strömungsdurchgang (8), der mit dem ersten Strömungsdurchgang (9) stromabwärts davon verbunden ist, wobei der zweite kapillare Strömungsdurchgang (8) einen im wesentlichen rechteckigen Querschnitt hat,
einen zweiten Einlaß (7) für ein Probenfluid,
eine Düse (10), die mit dem zweiten Einlaß (7) kommuniziert und sich innerhalb des ersten Strömungsdurchganges (9) in derselben Richtung wie der Strömungsrichtung des zweiten geraden kapillaren Strömungsdurchganges (8) öffnet,
eine Ausgabeöffnung (3), die an einem Anschlußende des zweiten geraden kapillaren Strömungsdurchganges (8) vorgesehen ist,
gekennzeichnet durch
eine Strömungsreguliereinrichtung zum Regulieren der Strömung des Mantelfluids in dem zweiten kapillaren Strömungsdurchgang (8) zu einer laminaren Strömung mit einem Gradienten der Strömungsgeschwindigkeit, wobei sich die Geschwindigkeit über dem zweiten geraden kapillaren Strömungsdurchgang (8) von der ersten Seitenwand (8a) zu der zweiten Seitenwand (8b) verringert, wobei die Strömungsreguliereinrichtung die zweite Seitenwand (8b) mit einer rauheren Oberfläche als die Oberfläche der ersten Seitenwand (8a) aufweist.

2. Durchflußzellenvorrichtung des Mantelströmungstyps gemäß Anspruch 1, wobei die Strömungsreguliereinrichtung des weiteren ein Teil (17) der oberen Wand (15) und ein Teil (18) der Bodenwand (16) des zweiten kapillaren Strömungsdurchganges (9) mit rauhen Oberflächenabschnitten neben der zweiten Seitenwand (8b) aufweist.

3. Durchflußzellenvorrichtung des Mantelströmungstyps gemäß Anspruch 1, wobei die Oberflächenrauigkeit der Oberfläche der ersten Seitenwand (8a) 1/500 und darunter einer Entfernung zwischen der ersten Seitenwand (8a) und der zweiten Seitenwand (8b) ist, und die Oberflächenrauigkeit der Oberfläche der zweiten Seitenwand (8b) 1/20 und darüber dieses Abstandes ist.

4. Durchflußzellenvorrichtung des Mantelströmungstyps gemäß Anspruch 1, wobei die Oberflächenrauigkeit der Oberfläche der ersten Seitenwand (8a) von 1S bis 10S beträgt, und die Oberflächenrauigkeit der Oberfläche der zweiten Seitenwand (8b) von 100S bis 1000S beträgt.

5. Durchflußzellenvorrichtung des Mantelströmungstyps gemäß Anspruch 2, wobei die Breite der rauhen Oberflächen (17, 18) der oberen und der Bodenwand (15, 16) von der zweiten Seitenwand (8b) 1/3 und darunter eines Abstandes zwischen der ersten Seitenwand (8a) und der zweiten Seitenwand (8b) ist.

6. Durchflußzellenvorrichtung des Mantelströmungstyps für ein Strömungs-Zytometer, die aufweist:
einen ersten Einlaß (6) für ein Mantelfluid;
einen ersten Strömungsdurchgang (9), der mit dem ersten Einlaß (6) kommuniziert und stromabwärts zusammengezogen ist, wobei der erste Strömungsdurchgang (9) einen im wesentlichen rechteckigen Querschnitt und gegenüberliegende erste und zweite Seitenwände (21, 22) aufweist, die durch obere und Bodenwände verbunden sind, wobei die obere Wand transparent ist und so ausgelegt ist, daß durch sie eine Messung von Streulicht und Fluoreszenz ermöglicht wird,
einen zweiten geraden kapillaren Strömungsdurchgang (8), der mit dem ersten Strömungsdurchgang (9) stromabwärts davon verbunden

ist, wobei der zweite kapillare Strömungsdurchgang (8) einen im wesentlichen rechteckigen Querschnitt aufweist, einen zweiten Einlaß (7) für ein Probenfluid, eine Düse (10), die mit dem zweiten Einlaß (7) kommuniziert und sich innerhalb des ersten Strömungsdurchganges (9) in der gleichen Richtung wie die Strömungsrichtung des zweiten geraden kapillaren Strömungsdurchganges (8) geöffnet ist,

eine Ausgabeöffnung (3), die an einem Anschlußende des zweiten geraden kapillaren Strömungsdurchganges (8) vorgesehen ist,

gekennzeichnet durch

eine Strömungsreguliereinrichtung zum Regulieren der Strömung des Mantelfluids in dem zweiten geraden kapillaren Strömungsdurchgang (8) zu einer laminaren Strömung mit einem Gradienten der Strömungsgeschwindigkeit, wobei sich die Geschwindigkeit über dem zweiten geraden kapillaren Strömungsdurchgang von der ersten Seitenwand (21) zu der zweiten Seitenwand (22) abnimmt, wobei die Strömungsreguliereinrichtung ein Netz (19) aufweist, das über dem ersten Strömungsdurchgang (9) stromaufwärts von der Öffnung der Düse (10) gespannt ist, wobei die Maschung des Netzes (19) sehr gering von der ersten Seitenwand (21) des ersten Strömungsdurchganges (9) in Richtung auf die zweite Seitenwand (22) gegenüber der ersten Seitenwand (21) ist.

7. Durchflußzellenvorrichtung des Mantelströmungstyps für ein Strömungs-Zytometer, die aufweist:

einen ersten Einlaß (6) für ein Mantelfluid; einen ersten Strömungsdurchgang (9), der mit dem ersten Einlaß (6) kommuniziert und stromabwärts zusammengezogen ist, wobei der erste Strömungsdurchgang (9) einen im wesentlichen rechteckigen Querschnitt und gegenüberliegende erste und zweite Seitenwände (22, 21) aufweist, die durch obere und Bodenwände verbunden sind, wobei die obere Wand transparent ist und so ausgelegt ist, daß durch sie eine Messung von Streulicht und Fluoreszenz ermöglicht wird,

einen zweiten geraden kapillaren Strömungsdurchgang (8), der mit dem ersten Strömungsdurchgang (9) stromabwärts davon verbunden ist, wobei der zweite kapillare Strömungsdurchgang (8) einen im wesentlichen rechteckigen Querschnitt aufweist,

einen zweiten Einlaß (7) für ein Probenfluid, eine Düse (10), die mit dem zweiten Einlaß (7) kommuniziert und innerhalb des ersten Strömungsdurchganges (9) in der gleichen Rich-

tung wie die Strömungsrichtung des zweiten kapillaren Strömungsdurchganges (8) geöffnet ist,

eine Ausgabeöffnung (3), die an einem Anschlußende des zweiten kapillaren Strömungsdurchganges (8) vorgesehen ist,

gekennzeichnet durch

eine Strömungsreguliereinrichtung zum Regulieren der Strömung des Mantelfluids in dem zweiten geraden kapillaren Strömungsdurchgang (8) zu einer laminaren Strömung mit einem Gradienten einer Strömungsgeschwindigkeit, wobei sich die Geschwindigkeit über dem geraden kapillaren Strömungsdurchgang von der ersten Seitenwand (22) zu der zweiten Seitenwand (21) verringert, wobei die Strömungsreguliereinrichtung eine Vielzahl von Unterteilungswänden (20) aufweist, die sich in dem ersten Strömungsdurchgang (9) in der Strömungsrichtung erstrecken und ihn in eine Vielzahl von unterteilten Strömungsdurchgängen (23a, 23b, 23c, 23d, 23e, 23f) unterteilen, deren Längen größer ausgeführt sind von der ersten Seitenwand (22) des ersten Strömungsdurchganges (9) in Richtung auf die zweite Seitenwand (21) gegenüber der ersten Seitenwand (22), um den Strömungswiderstand von der ersten Seitenwand (22) in Richtung auf die zweite Seitenwand (21) größer zu machen.

Revendications

1. Un appareil à cellule d'écoulement du type à écoulement enveloppant pour un cytomètre à écoulement, comprenant :

une première entrée (6), pour le fluide d'enveloppement,

un premier passage d'écoulement (9), communiquant avec cette première entrée (6) et allant en se restreignant vers l'aval, ce premier passage d'écoulement (9) présentant une section droite essentiellement rectangulaire et faisant face à une première et à une seconde paroi latérales (8a, 8b) reliées par des parois supérieure et inférieure (15, 16), la paroi supérieure étant transparente et conçue de manière à permettre une mesure à son travers de la lumière dispersée et de la fluorescence,

un second passage d'écoulement capillaire étroit (8), relié au premier passage d'écoulement (9) en aval de celui-ci, ce second passage d'écoulement capillaire (8) présentant une section droite essentiellement rectangulaire,

une seconde entrée (7), pour un fluide échantillon,

une buse (10), communiquant avec cette seconde entrée (7) et s'ouvrant dans le premier passage d'écoulement (9) dans le même

sens que le sens d'écoulement du second passage d'écoulement capillaire étroit (8),

un orifice d'évacuation (3), disposé à une extrémité terminale du second passage d'écoulement capillaire étroit (8),

caractérisé par

des moyens régulateurs de débit, pour réguler le débit du fluide d'enveloppement dans le second passage d'écoulement capillaire (8) de manière à obtenir un écoulement laminaire présentant un gradient de vitesse d'écoulement, cette vitesse diminuant sur l'étendue du second passage d'écoulement capillaire étroit (8) depuis la première paroi latérale (8a) jusqu'à la seconde paroi latérale (8b), ces moyens régulateurs de débit comprenant le fait que la seconde paroi latérale (8b) possède une surface plus rugueuse qu'une surface de la première paroi latérale (8a).

2. Un appareil à cellule d'écoulement du type à écoulement enveloppant selon la revendication 1, dans lequel les moyens régulateurs de débit comprennent en outre le fait qu'une partie (17) de la paroi supérieure (15) et une partie (18) de la paroi inférieure (16) du second passage d'écoulement capillaire (9) présentent des portions de surface rugueuse au voisinage de la seconde paroi latérale (8b).
3. Un appareil à cellule d'écoulement du type à écoulement enveloppant, dans lequel la rugosité de surface de ladite surface de la première paroi latérale (8a) est de 1/500 et sous une distance comprise entre la première paroi latérale (8a) et la seconde paroi latérale (8b), et la rugosité de surface de ladite surface de la seconde paroi latérale (8b) est de 1/20 et au-dessus de cette distance.
4. Un appareil à cellule d'écoulement du type à écoulement enveloppant, dans lequel la rugosité de surface de ladite surface de la première paroi latérale (8a) existe de 1S à 10S et la rugosité de surface de ladite surface de la seconde paroi latérale (8b) existe de 100S à 1000S.
5. Un appareil à cellule d'écoulement du type à écoulement enveloppant, dans lequel la largeur des surfaces rugueuses (17, 18) des parois supérieure et inférieure (15, 16) depuis la seconde paroi latérale (8b) est d'1/3 et sous une distance comprise entre la première paroi latérale (8a) et la seconde paroi latérale (8b).
6. Un appareil à cellule d'écoulement du type à écoulement enveloppant pour un cytomètre à

écoulement, comprenant :

une première entrée (6), pour le fluide d'enveloppement,

un premier passage d'écoulement (9), communiquant avec cette première entrée (6) et allant en se restreignant vers l'aval, ce premier passage d'écoulement (9) présentant une section droite essentiellement rectangulaire et faisant face à une première et à une seconde paroi latérales (21, 22) reliées par des parois supérieure et inférieure, la paroi supérieure étant transparente et conçue de manière à permettre une mesure à son travers de la lumière dispersée et de la fluorescence,

un second passage d'écoulement capillaire étroit (8), relié au premier passage d'écoulement (9) en aval de celui-ci, ce second passage d'écoulement capillaire (8) présentant une section droite essentiellement rectangulaire,

une seconde entrée (7), pour un fluide échantillon,

une buse (10), communiquant avec cette seconde entrée (7) et s'ouvrant dans le premier passage d'écoulement (9) dans le même sens que le sens d'écoulement du second passage d'écoulement capillaire étroit (8),

un orifice d'évacuation (3), disposé à une extrémité terminale du second passage d'écoulement capillaire étroit (8),

caractérisé par

des moyens régulateurs de débit, pour réguler le débit du fluide d'enveloppement dans le second passage d'écoulement capillaire (8) de manière à obtenir un écoulement laminaire présentant un gradient de vitesse d'écoulement, cette vitesse diminuant sur l'étendue du second passage d'écoulement capillaire étroit depuis la première paroi latérale (21) jusqu'à la seconde paroi latérale (22), ces moyens régulateurs de débit comprenant un organe formant filet (19) étiré sur l'étendue du premier passage d'écoulement (9) en amont de l'ouverture de la buse (10), l'écartement entre mailles de cet organe formant filet (19) allant en se resserrant depuis la première paroi latérale (21) du premier passage d'écoulement (9) en direction de la seconde paroi latérale (2) en vis-à-vis de cette première paroi latérale (21).

7. Un appareil à cellule d'écoulement du type à écoulement enveloppant pour un cytomètre à écoulement, comprenant :

une première entrée (6), pour le fluide d'enveloppement,

un premier passage d'écoulement (9), communiquant avec cette première entrée (6) et allant en se restreignant vers l'aval, ce premier passage d'écoulement (9) présentant une

section droite essentiellement rectangulaire et faisant face à une première et à une seconde paroi latérales (22, 21) reliées par des parois supérieure et inférieure, la paroi supérieure étant transparente et conçue de manière à permettre une mesure à son travers de la lumière dispersée et de la fluorescence,

un second passage d'écoulement capillaire étroit (8), relié au premier passage d'écoulement (9) en aval de celui-ci, ce second passage d'écoulement capillaire (8) présentant une section droite essentiellement rectangulaire,

une seconde entrée (7), pour un fluide échantillon,

une buse (10), communiquant avec cette seconde entrée (7) et s'ouvrant dans le premier passage d'écoulement (9) dans le même sens que le sens d'écoulement du second passage d'écoulement capillaire étroit (8),

un orifice d'évacuation (3), disposé à une extrémité terminale du second passage d'écoulement capillaire étroit (8),

caractérisé par

des moyens régulateurs de débit, pour réguler le débit du fluide d'enveloppement dans le second passage d'écoulement capillaire (8) de manière à obtenir un écoulement laminaire présentant un gradient de vitesse d'écoulement, cette vitesse diminuant sur l'étendue du second passage d'écoulement capillaire étroit depuis la première paroi latérale (22) jusqu'à la seconde paroi latérale (21), ces moyens régulateurs d'écoulement comprenant une pluralité de parois de séparation (20) s'étendant dans le premier passage d'écoulement (9) dans le sens d'écoulement et divisant celui-ci en une pluralité de passages d'écoulement divisés (23a, 23b, 23c, 23d, 23e, 23f) dont les longueurs sont rendues croissantes depuis la première paroi latérale (22) du premier passage d'écoulement (9) jusqu'à la seconde paroi latérale (21) en vis-à-vis de cette première paroi latérale (22), afin de procurer une résistance à l'écoulement croissante depuis la première paroi latérale (22) jusqu'à la seconde paroi latérale (21).

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FIG. 1

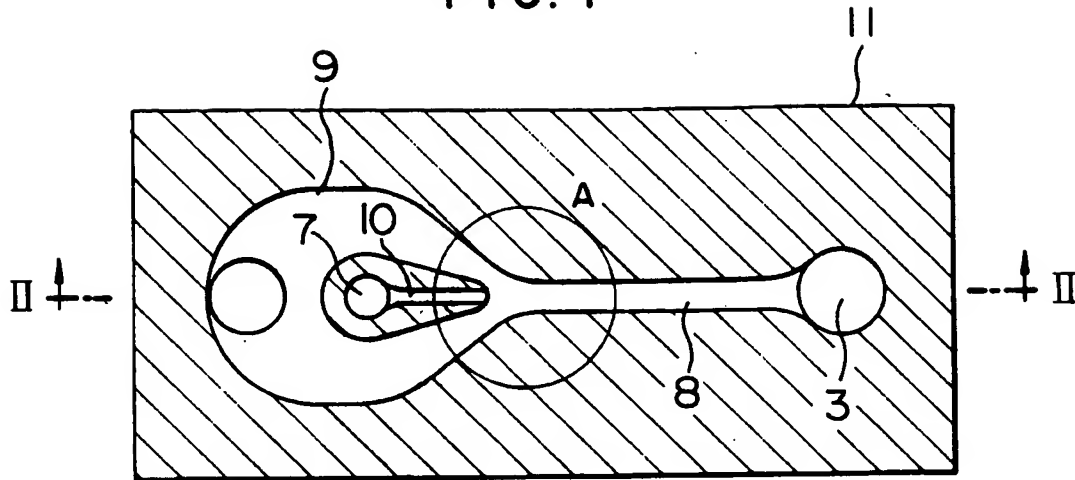


FIG. 2

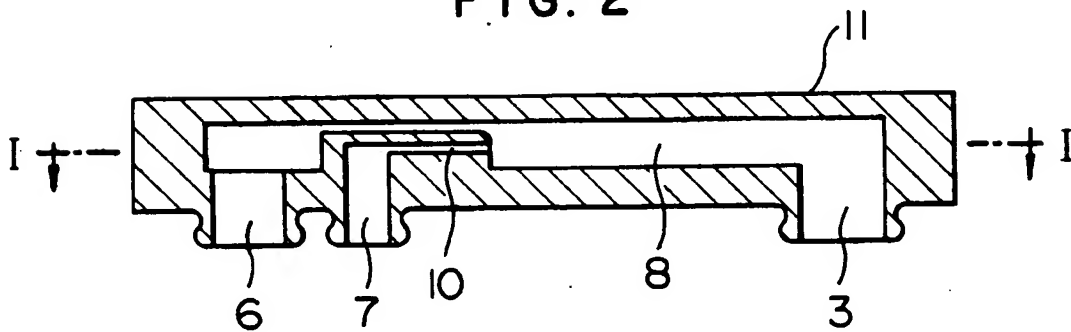


FIG. 3

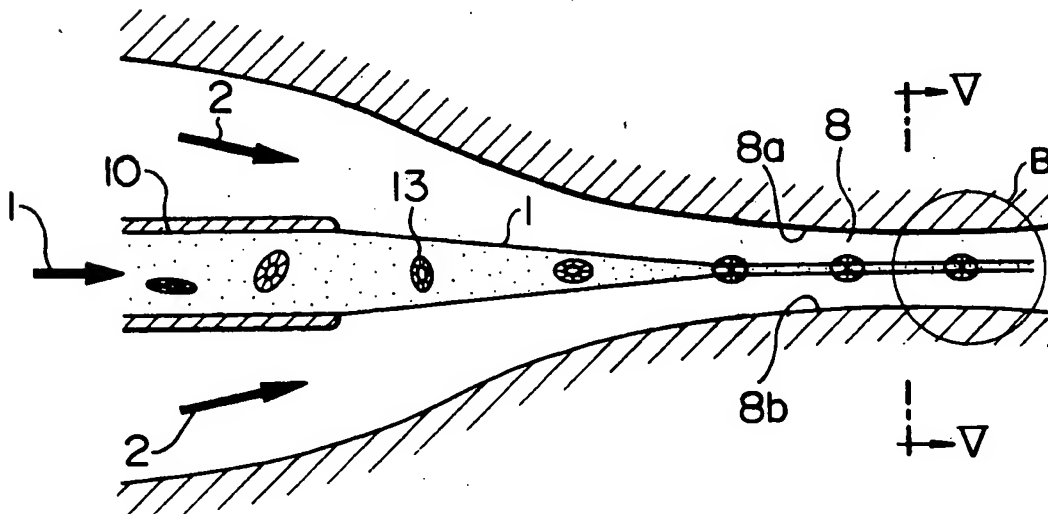


FIG. 4

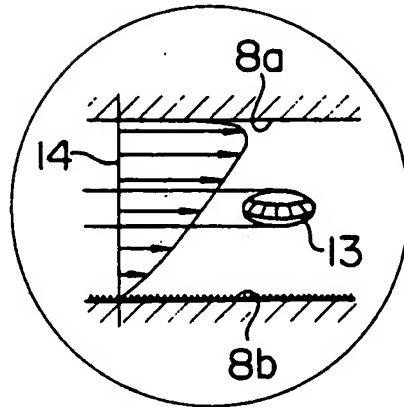


FIG. 5

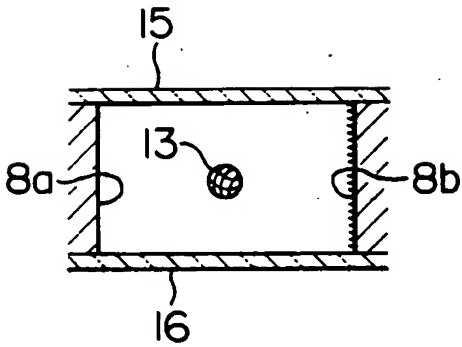


FIG. 6

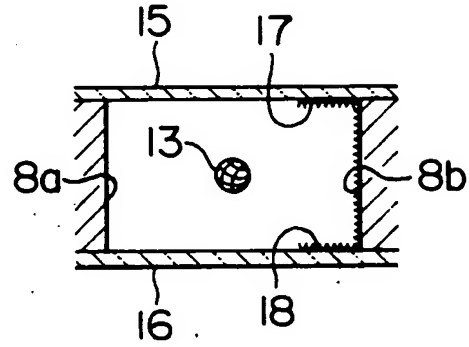


FIG. 7

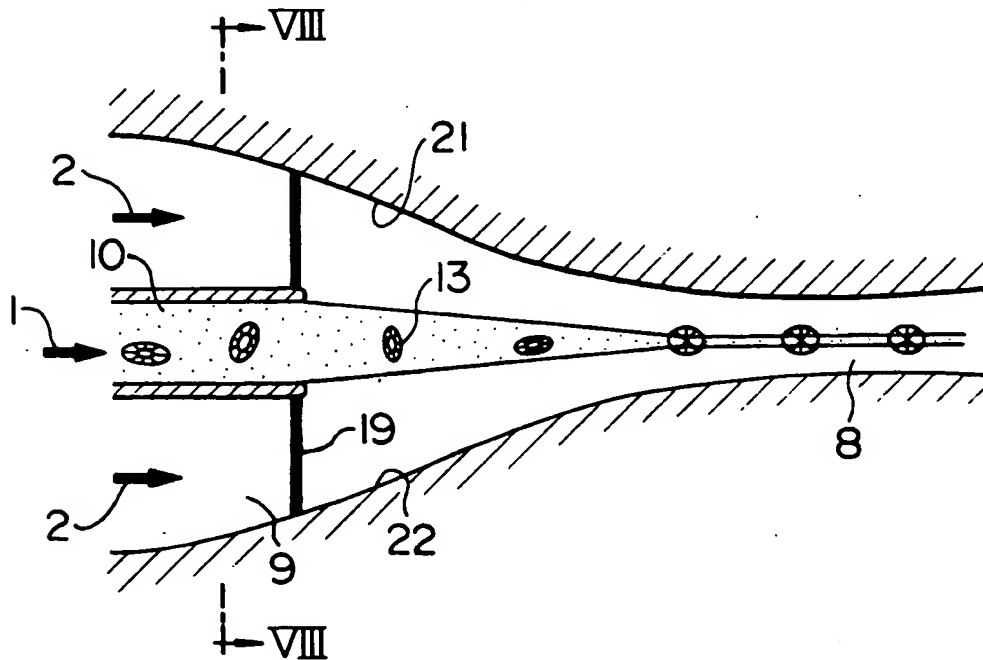


FIG. 8

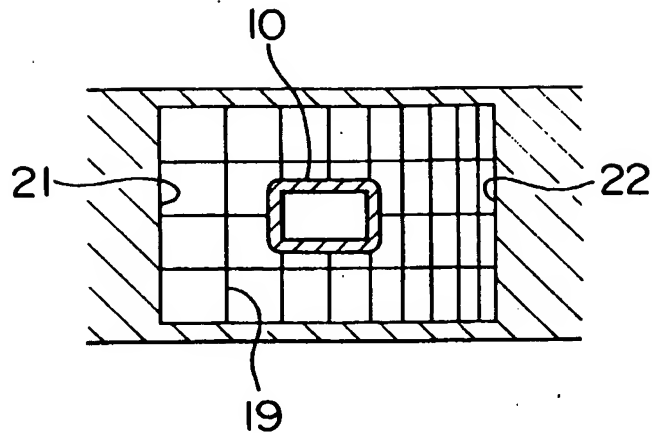


FIG. 9

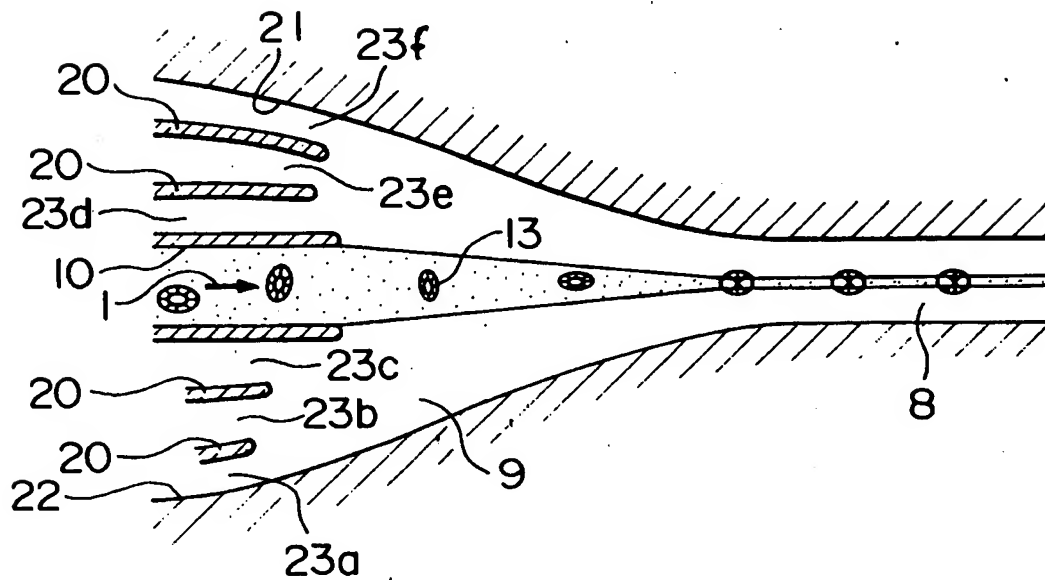


FIG. 10
PRIOR ART

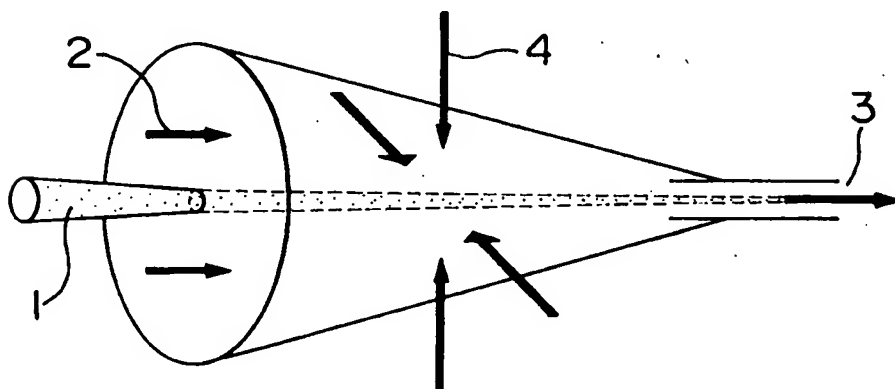


FIG. II
PRIOR ART

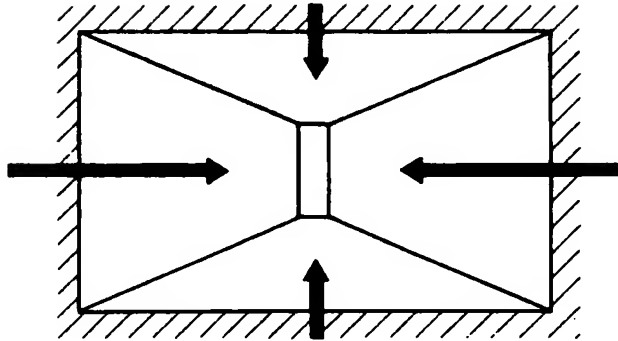


FIG. 12A
PRIOR ART

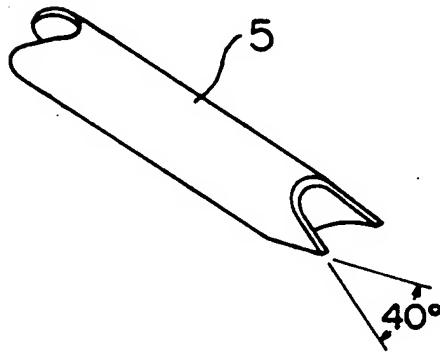


FIG. 12B
PRIOR ART

